## Artifact-Resistant Motion Estimation for Motion-Compensated CT

#### Marcus Brehm<sup>1,2</sup>, <u>Thorsten Heußer</u><sup>1</sup>, Pascal Paysan<sup>3</sup>, Markus Oehlhafen<sup>3</sup>, and Marc Kachelrieß<sup>1,2</sup>

<sup>1</sup>German Cancer Research Center (DKFZ), Heidelberg, Germany <sup>2</sup>Friedrich-Alexander-University (FAU) Erlangen-Nürnberg, Germany <sup>3</sup>Varian Medical Systems Imaging Laboratory, Baden-Dättwil, Switzerland







## **Slowly Rotating CBCT Devices**

#### Image-guided radiation therapy (IGRT)

- CBCT imaging unit mounted on gantry of a LINAC treatment system
- E.g. used for patient positioning
- Maximum gantry rotation speed of 6° per second
- Breathing cycle about 2 to 5 seconds
  - i.e. 12 to 30 respirations per minute (rpm) and thus per scan



#### $\Rightarrow$ Account for respiratory motion!



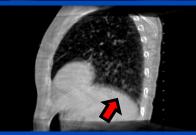


## **Retrospective Gating**

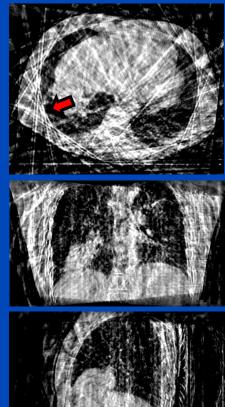
#### Without gating (3D): Motion artifacts

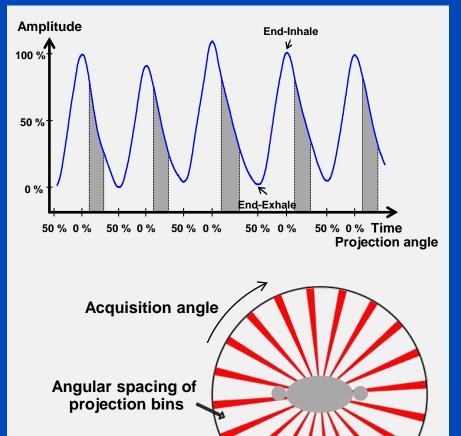






#### With gating (4D): Sparse-view artifacts





Measured projections assigned to one phase bin

VAR AN medical systems



### **Prior Art in IGRT** (Respiratory-Correlated Reconstructions)

#### Respiratory gating and independent reconstruction

- Sparse-view artifacts deteriorate image quality
  - » Streak artifacts and image noise
- Increased patient dose required

#### Dedicated acquisition techniques

- These are not accepted in clinical routine, e.g., due to long acquisition times
- Increased patient dose required

#### Conventional motion-compensated reconstruction

- Necessary motion estimation requires
  - » Increased patient dose
  - » Additional knowledge, e.g. planning CT



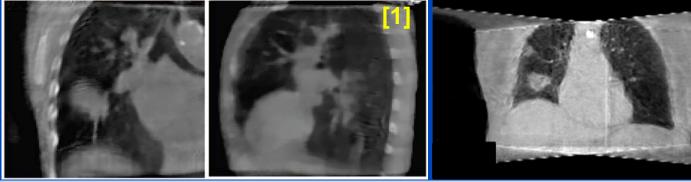


## Aim

- Provide high quality respiratory-correlated 4D volumes from on-board CBCT scans
  - Image quality comparable to that of motionless regions (e.g. neck)
- Do this with a standard acquisition protocol
- Do this without other prior information of higher temporal sampling such as a 4D planning CT
  - Account for inter-fractional variations in breathing motion

#### Results of recent publications from other groups on that topic

2



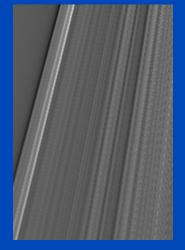
 [1] Wang and Gu, Simultaneous motion estimation and image reconstruction (SMEIR) for 4D cone-beam CT, Medical Physics 40(10):101912 (2013).
 [2] Christoffersen, Hansen, Poulsen, and Sørensen, Registration-based reconstruction of four-dimensional cone beam computed tomography, IEEE Transactions on Medical Imaging 32(11):2064-2077 (2013).

## Motion Compensation (MoCo)

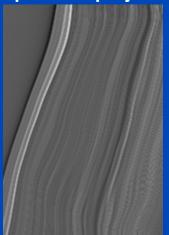
#### Straight backprojection

#### Use all projection data for each phase to be reconstructed

- Even those of other phase bins (100 % dose usage)
- Compensate for motion using motion vector fields (MVFs)
- In our case MVFs are estimated from gated reconstructions
- Use MVFs during reconstruction
  - Backproject sparse data along straight lines, then warp with respect to the MVFs



Warped backprojection

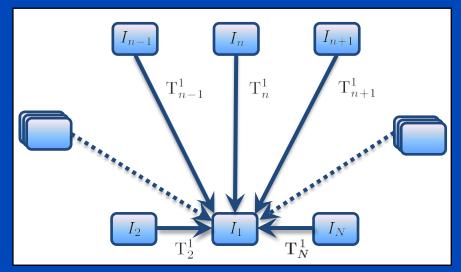






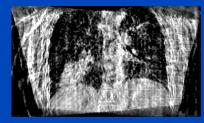
## A Standard Motion Estimation and Compensation Approach (sMoCo)

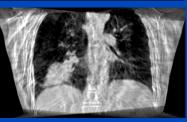
#### Motion estimation via standard 3D-3D registration

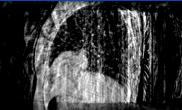


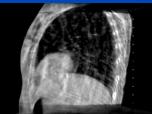
Has to be repeated for each reconstructed phase

# Gated 4D CBCT sMoCo Image: SMoCo Image: SMoCo









 Streak artifacts from gated reconstructions propagate into sMoCo results

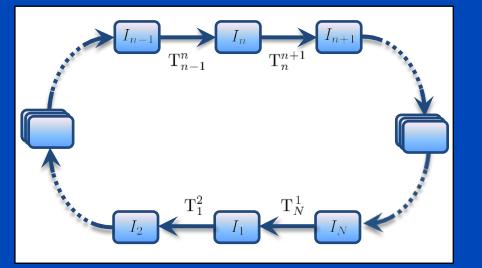


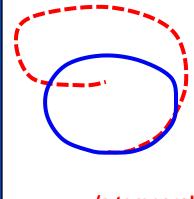
Li et al., "Enhanced 4D cone-beam CT with inter-phase motion model," Med. Phys. 51(9), 3688-3695 (2007).



## A Cyclic Motion Estimation and Compensation Approach (cMoCo)

• Motion estimation only between adjacent phases – All other MVFs given by concatenation





Displacement curve of a fictitious pixel over complete respiratory cycle

w/o temporal constraints
with temporal constraints

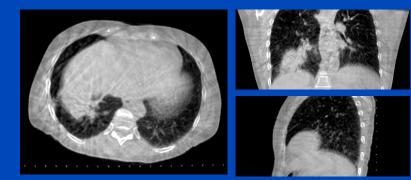
- Incorporate additional knowledge
  - A priori knowledge of quasi periodic breathing pattern
  - Non-cyclic motion is penalized
  - Error propagation due to concatenation is reduced

Brehm, Paysan, Oelhafen, Kunz, and Kachelrieß, "Self-adapting cyclic registration for motion-compensated cone-beam CT in image-guided radiation therapy," Med. Phys. 39(12), 7603-7618 (2012). Reported at CT-Meeting 2012, MIC 2012, RSNA 2012.

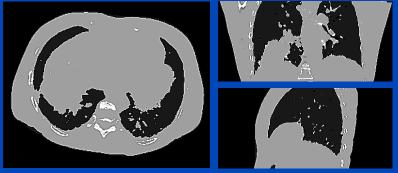


## **Angular Sampling Artifact Model**

- Create second series of images with sparse-view artifacts but without breathing motion
- Eliminate breathing motion information
  - Threshold-based segmentation of 3D CBCT
- Simulate measurement and reconstruction process
  - Forward projection of segmented image
  - Backprojection at same angles as for gated 4D CBCT



**3D CBCT** 



#### **Segmented Image**

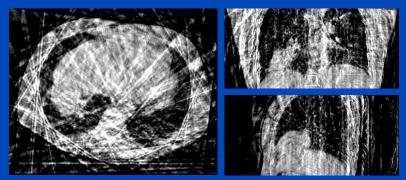


C = -200 HU, W = 1400 HU

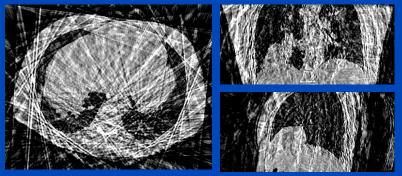


## **Angular Sampling Artifact Model**

- Create second series of images with sparse-view artifacts but without breathing motion
- Eliminate breathing motion information
  - Threshold-based segmentation of 3D CBCT
- Simulate measurement and reconstruction process
  - Forward projection of segmented image
  - Backprojection at same angles as for gated 4D CBCT



Gated 4D CBCT



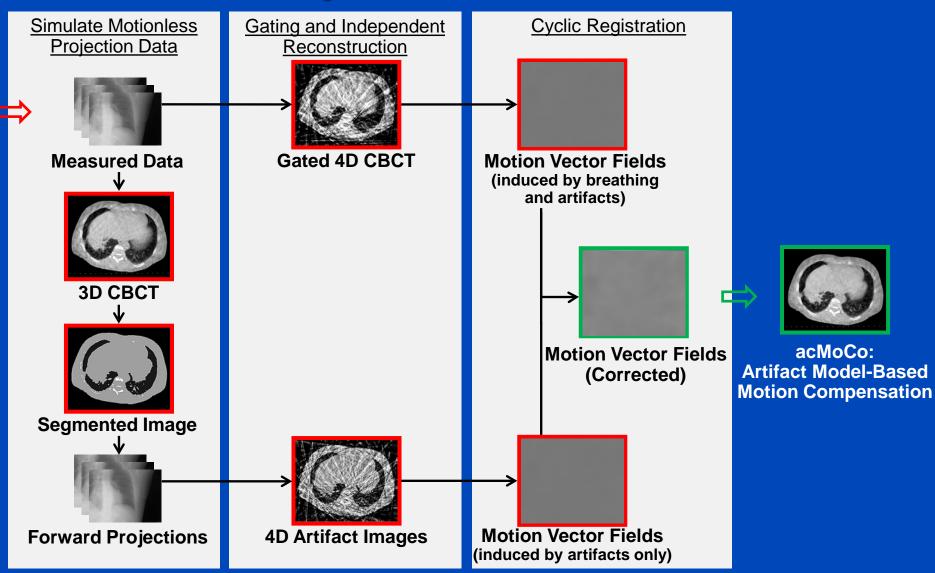
#### **4D Artifact Images**



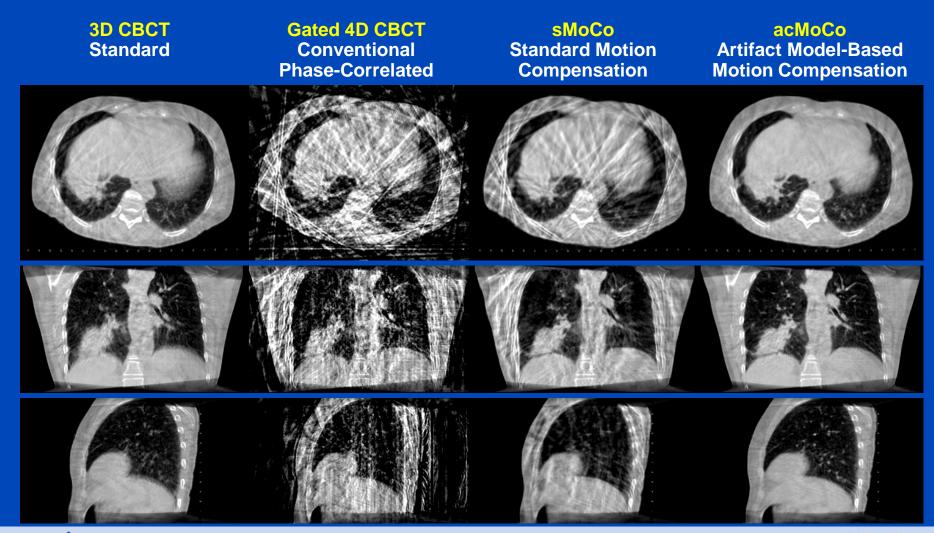
C = -200 HU, W = 1400 HU



## Motion Estimation using an Patient-Specific Artifact Model



## Patient Data – Results



C = -200 HU, W = 1400 HU

VARIAN

medical systems



## Summary

- Severe sparse-view artifacts deteriorate image quality of conventional phase-correlated images.
- Standard deformable 3D-3D registration is sensitive to these artifacts.
- Highly decreased sensitivity to sparse-view artifacts by combination of cyclic registration and artifact model.
- Motion-compensated image reconstruction using MVFs obtained by combination of cyclic registration and artifact model appears to be suitable for application in IGRT.





# Thank You!

# This study was supported by a research grant from Varian Medical Systems, Palo Alto, CA.

This presentation will soon be available at www.dkfz.de/ct.

Parts of the reconstruction software were provided by RayConStruct<sup>®</sup> GmbH, Nürnberg, Germany.



