Estimating the High Scatter Frequencies Caused by Coarse Anti-Scatter Grids in X-Ray CT

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Photon-Counting enables Visualization of Small Details



Reconstruction to mimick conventional energy-integrating CT, e.g. Somatom Flash



Reconstruction of data scanned at photon-counting CT Naoetom Alpha



Properties of Photon-Counting Detectors

Smaller detector pixels

- can deliver ultra high resolution imaging
- less dose due for conventional spatial resolution¹ ("small pixel effect")
- No electronic noise
 - advanced image quality in obese patients and low-dose scans
- No downweighting of lower energy quanta
 - improved image contrast
 - less dose due to increased iodine CNR² ("iodine effect")
- Intrinsic spectral sensitivy
 - established dual energy applications available in any scan

[1] Klein, Kachelrieß, Sawall et al. "Effects of Detector Sampling on Noise Reduction in Clinical Photon-Counting Whole-Body Computed Tomography." *Investigative Radiology* vol. 55(2): 111-119, 2020.

[2] Sawall, Kachelrieß et al. "Iodine Contrast-to-Noise Ratio Improvement at Unit Dose and Contrast Media Volume Reduction in Whole-Body Photoncounting CT." *European Journal of Radiology* vol. 126: 108909, 2020.





Scatter for Coarse ASG



Coarse ASG leads to changing scatter intensity between neighboring pixel depending on the incident angle of the photon





Scatter for Coarse ASG

Scatter distribution averaged over all detector rows



Healthineers

Scatter for Coarse ASG



Healthineers



Scatter Artifacts of Coarse ASG



Coarse ASG can lead to scatter-induced moiré artifacts.



Reconstruction: C = 40 HU, W = 300 HU



Deep Scatter Estimation (DSE)

- Use a deep convolutional neural network to estimate scatter using the • acquired projection data as input.^{1,2}
- Train the network to predict Monte Carlo scatter estimates based on the • acquired projection data.^{1,2}
- DSE outperforms other scatter estimation techniques.^{1,2,4,5} •
- DSE is much faster than the Monte Carlo simulation.^{1,2,5} •
- DSE can also be trained with measured scatter data.³ •
- DSE shows great potential to correct for cross-scatter in dual source CT.4,5 •



- [1] J. Maier, M. Kachelrieß et al. "Deep Scatter Estimation (DSE)", SPIE 2017 and J. of Nondest. Eval. 37:57, July 2018.
- [2] J. Maier, M. Kachelrieß et al. "Robustness of DSE", Med. Phys. 46(1):238-249, January 2019.
- [3] J. Erath, M. Kachelrieß et al "Monte-Carlo-Free Deep Scatter Estimation (DSE) for X-Ray CT and CBCT", RSNA 2019
- [4] J. Erath, T. Vöth, J. Maier, E. Fournié, M. Petersilka, K. Stierstorfer, and M. Kachelrieß, "Deep Scatter Correction in DSCT", CT Meeting August 2020.
 [5] J. Erath, T. Vöth, J. Maier, E. Fournié, M. Petersilka, K. Stierstorfer, and M. Kachelrieß, "Deep Learning-Based Forward and Cross-Scatter Correction in DS CT" Med. Phys. 2021



Matrix Multiplication

- To obtain scatter via MC simulation for every subpixel comes with high computational costs
- How accurate can neural network estimate scatter with additional pattern on it?
- Idea: multiply scatter data with pattern matrix
- 1. Matrix multiplication with ones:
 - e, b, a, d, c = 1
- 2. Matrix multiplication with constant values:
 - e = b = 1, a = d = 0.8, c = 0.6
- 3. Matrix multiplication with random values :
 - e = b = 1, 0.7 < a = d < 0.9, 0.4 < c < 0.7
 - After each projection new random matrix
- Detector size 1024 × 128

Healthineer

• First and last row multiplied with 1 (126 divisible by 6)





Results in Projection Domain

| Matrix o | ones _{GT} | |
|--------------------|-------------------------------|--|
| | Prediction | |
| | Difference GT - Prediction | |
| Matrix constant | GT | |
| | Prediction | |
| | Difference GT - Prediction | |
| Matrix random | GT | |
| | Prediction | |
| | Difference GT - Prediction | |

GT & Prediction: *C* = 0.0004, *W* = 0.0008

Difference: C = 0.0000, W = 0.0008



Results Matrix = 1



SIEMENS Images: C = 40 HU, W = 300 HU Differences: C = 0 HU, W = 300 HU

Results Matrix = 1



SIEMENS Healthineers Images: C = 40 HU, W = 300 HU Differences: C = 0 HU, W = 300 HU

Results Matrix Constant



SIEMENS Images: C = 40 HU, W = 300 HU Differences: C = 0 HU, W = 300 HU

Results Matrix Constant



SIEMENS Healthineers Images: C = 40 HU, W = 300 HU Differences: C = 0 HU, W = 300 HU

Results Matrix Random



Uncorrected MAE = 11.0 HU



DSE 2D MAE = 2.0 HU





SIEMENS Images: C = 40 HU, W = 300 HU Differences: C = 0 HU, W = 300 HU

Results Matrix Random



SIEMENS Healthineers : C = 40 HU, W = 300 HU Differences: C = 0 HU, W = 300 HU

Conclusions

- Smaller detector pixel and coarse anti-scatter grid can lead to moiré artifacts.
- Scatter induced moiré effect can be corrected with deep learning-based scatter correction.
- Neural network is able to detect additional pattern on scatter.
- With the proposed algorithm the mean absolute error (MAE) could be reduced from uncorrected about 10 HU to about 1 HU.
- The amplitude of the scatter induced moiré effect can be corrected from 20 HU to less than 1 HU.
- Next step: apply matrix deep-learning based correction for measurements.

This presentation will soon be available at www.dkfz.de/ct. Job opportunities through DKFZ's international PhD or Postdoctoral Fellowship programs (marc.kachelriess@dkfz.de).

