



FACULTY OF ENGINEERING

Towards Automatic Abdominal Multi-Organ Segmentation in Dual Energy CT using Cascaded 3D Fully Convolutional Network

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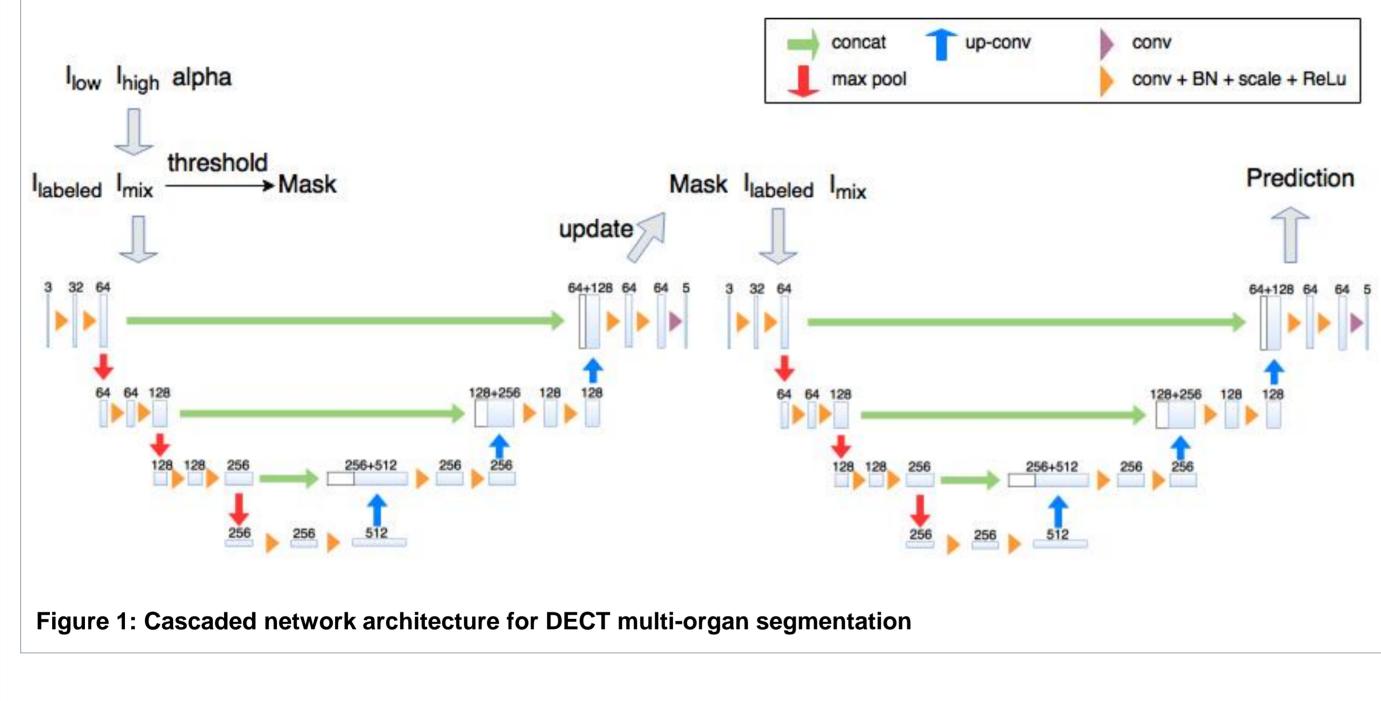
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Introduction

- Use dual energy information to improve segmentation accuracy
- First study about automatic multi-organ segmentation on dual energy computed tomography (DECT) images using deep learning
- Based on a cascaded 3D fully convolutional network (FCN) [1]

Material and Methods



Results and Discussion

- Experiment setup:
- 42 clinical torso DECT images
- Voxel dimensions: [0.6895-0.959, 0.6895-0.959, 0.6] mm
- 30 for training, 6 for validation, 6 for test, data selected using a manifold learning-based technique [3]
- Data augmentation: rotation, elastic deformation
- Results:
- Best results with optimal α : liver 0.93, spleen 0.92, right kidney 0.91, left kidney 0.89
- SECT results:

Image fusion in the preprocessing based on linear weighting [2]: $I_{mix} = \alpha \cdot I_{low} + (1 - \alpha) \cdot I_{hiah}$

-> to merge the images of different energies

- **Binary mask generation** based on thresholding -> to undersample the background for the high class imbalance problem
- Cascaded end-to-end network (Figure 1):
 - Stage 1: calculation of the region of the interest (ROI)

-> to further undersample the background and oversample the minor classes

- -> to improve the class weights
- -> ROI is used as mask for the stage 2
- Stage 2: calculation of the final class probability

-> High(α = 0): liver 0.91, spleen 0.88, right kidney 0.84, left kidney 0.85 -> Low(α = 1): liver 0.92, spleen 0.90, right kidney 0.88, left kidney 0.89

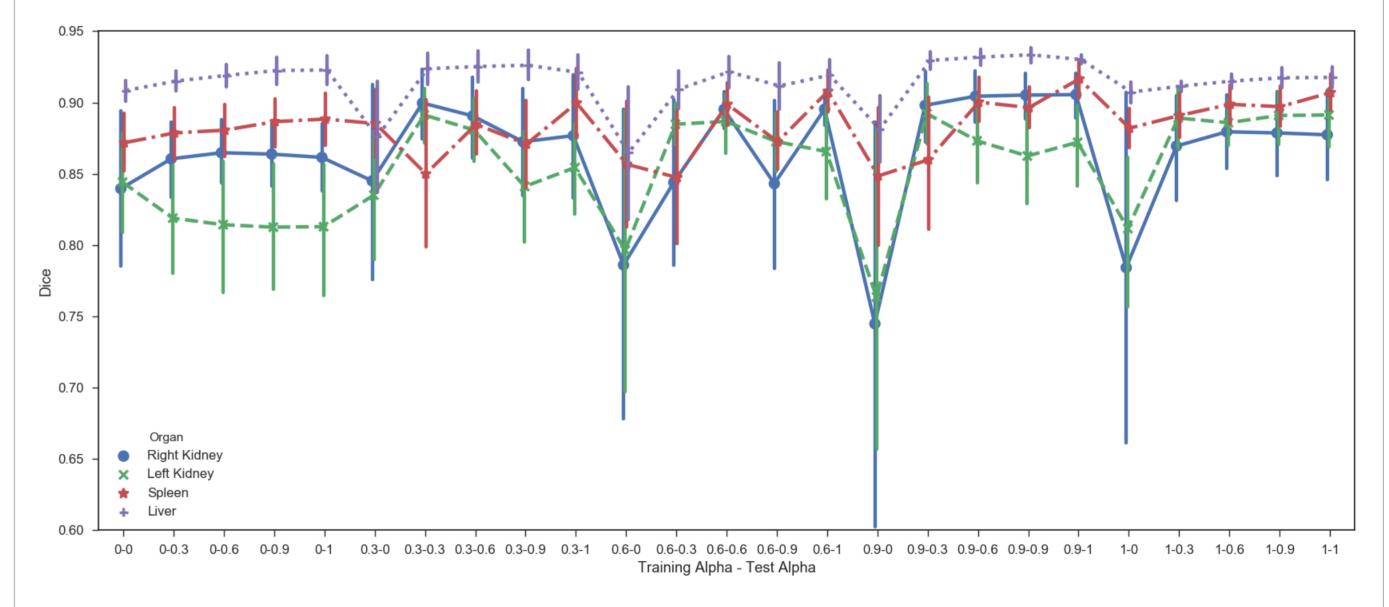


Figure 2: Evaluation with different α

Conclusion

- DECT accuracy with optimal α is higher than SECT ($\alpha = 0$ and $\alpha = 1$).
- Multi-organ segmentation on DECT using deep learning is promising and robust.
- Data sampling using manifold learning improves the accuracy.
- Image fusion factor α affects the accuracy.
- The optimal α is organ-different.

- Voxel-wise class balancing:
 - Weighted voxel-wise cross-entropy loss using softmax class probabilites p_k :
 - $L = \frac{-1}{N} \sum_{k=i}^{K} \lambda_i \times \left(\sum_{x \forall N_i} \log(\widehat{p_k}(x)) \right)$
 - Weight factor λ_i based on voxel number within ROI N_c [1]: $\lambda_i = \frac{1 - \frac{N_i}{N_c}}{N_c}$

References

- 1. Roth et al., "Hierarchical 3D fully convolutional networks for multi-organ segmentation," in arXiv preprint arXiv:1704.06382.
- 2. Krauss et al., Dual Energy CT in Clinical Practice, chapter Dual Source CT, Springer Berlin Heidelberg, 2011.
- 3. Chen et al., "Manifold learning-based data sampling for model training," Proce BVM, 2018, pp. 269–274.



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